# **Electronic Elements and Circuits**





©2010 Mark Cohen, all rights reserved

Voltage

Potential Energy from Charge AttractionSeparation of Charge results in Stored Energy



Electrical Potential energy is Measured in Volts (V) whose units are Joules/Coulomb

- Voltage is sometimes called, "Electromotive Force" or e.m.f.
- The notation for charge is Q

2010 Mark Cohen, all rights reserved

Medical Center





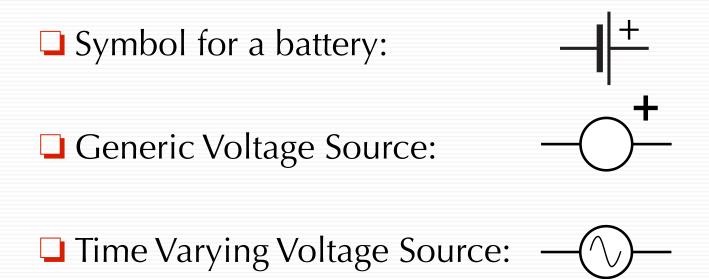
# **Voltage Sources**

Medical Center

2010 Mark Cohen, all rights reserved

Batteries store electrical potential energy by chemically separating ions

Salts separated across semi permeable membranes may be used as "batteries."





### Current

Electrical Kinetic Energy is called Current

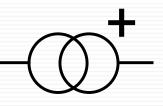
- Current is the motion of charge
- The Electrical Engineers symbol for current is *i* (\*).
- Current Flows "through" conductors
- Current is therefore *dQ/dt*

Medical Center

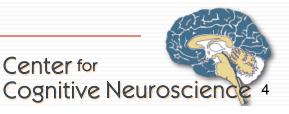
The Unit of Current is "Amperes" or amps.

Symbol for a current source:

Mark Cohen, all rights reserved



\* Hence, engineers use "j" to denote  $\sqrt{-1}$ 



- Current flowing through a path experiences *Resistance*.
- Less current flow through higher resistance:
  - Ohm's Law: i = V/R
  - Larger resistance -> less current
- Energy is dissipated (lost) to that resistance
- As charge flows the stored energy is dissipated
- The RATE of Energy dissipation is measured in Watts (power, Joules/second)
- iV = (Joules/coulomb)(coulombs/s) = Joules/s.

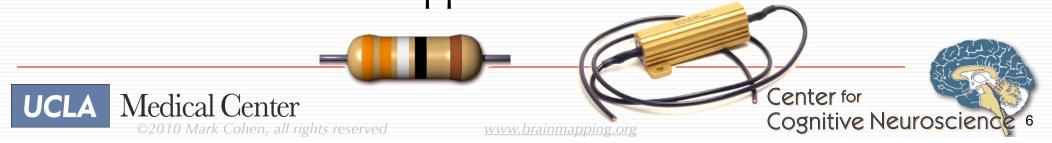




Insulators allow little or no current flow
 Conductors pass current easily.
 Conductor symbol:

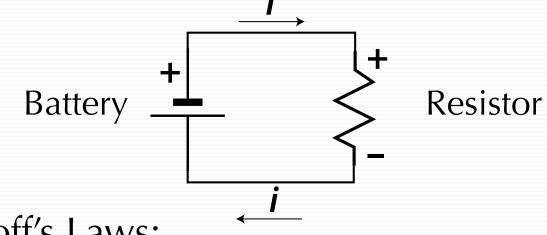
Typical "Resistors" range in values from about 1 Ohm to about 10E6 Ohm (10Megohm)
 □ resistor symbol: -∧ ∧

A 1 Ohm resistor allows 1 Ampere of current to flow when 1 Volt is applied across it.



Circuit

Circuits always show the complete path for current flow



Kirchhoff's Laws:

**KCL**: Current through any node adds to zero

any two terminal device is a node

- **KVL**: Voltage around any loop adds to zero
- Both laws are an expression of conservation of energy



# Series Circuit - Voltage Divider

In a series circuit **KVL** says that Vs = V1 + V2

**KCL** says that *i* is the same in R1 and R2

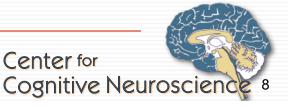
Ohms law states that  $V_1 = iR1$  and  $V_2 = iR2$ 

Therefore: Vs = i(R1+R2) +  $V_1$  -+ R1 +  $V_2$  +

It follows that  $V_2 = Vs (R2/(R1+R2))$ 

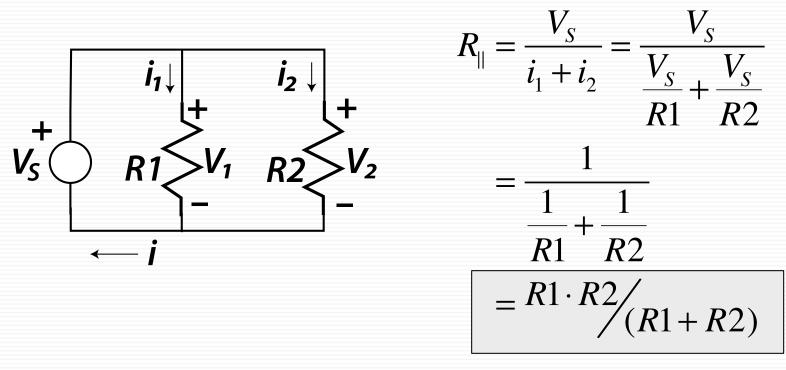


mapping.org



# Parallel Circuit = Current Divider

KCL says that *i* = *i*<sub>1</sub> + *i*<sub>2</sub>
 KVL says that V<sub>1</sub> =V<sub>2</sub>: Vs = *i*<sub>1</sub> R1 = *i*<sub>2</sub> R2
 The apparent resistance is: Vs/(*i*<sub>1</sub> + *i*<sub>2</sub>)

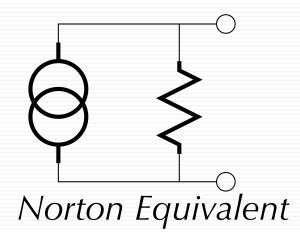


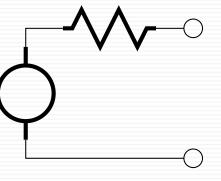




# Norton and Thévenin Equivalent

Real voltage and current sources have internal resistance





Thévenin Equivalent

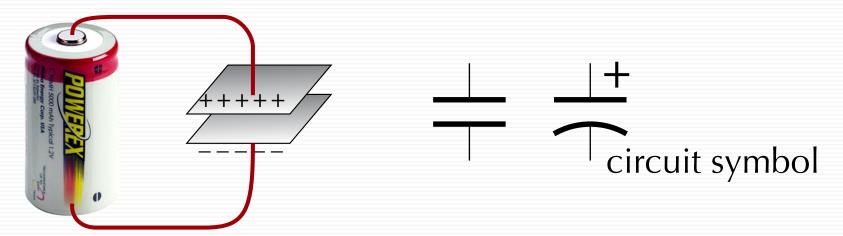
In a real current source, as Load resistance increases, current drops In a real voltage source, as Load resistance decreases, voltage drops



UCLA Medical Center ©2010 Mark Cohen, all rights reserved

Capacitor

When voltage is applied across an insulator charge moves onto the insulator.



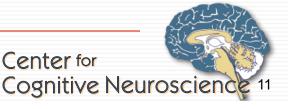
If the voltage source is removed, the separated charge stores potential energy

Capacitance measures the amount of energy stored by separated charge: C = Q/V

Capacitance is measured in Farads

Medical Center

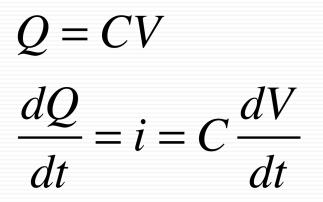
2010 Mark Cohen, all rights reserved



# Capacitor (cont'd)

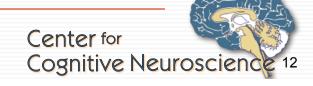
If charge is applied to one side of the capacitor, equal and opposite charge will move to the other side.

This results in a net current "through" the capacitor.



This appears similar to Ohm's law.





# Laplace Transform

Note that:  $d(Ae^{st}) = sAe^{st}$ 

- Finding the derivative of a function of the form *Ae*<sup>st</sup> is like multiplying by s
- Finding the integral is like dividing by s
- Applying the Laplace transform typically reduces differential equations to simple algebra.





Capacitors and Sinusoids

Let: 
$$V(t) = A\cos(\omega t)$$
:  
For a capacitor:  
 $i_c = C \frac{dv}{dt} = -\omega CA\sin(\omega t)$   
 $-\omega CA\sin(\omega t) = \omega CA\cos(\omega t - 90^\circ)$   
 $\frac{V}{i_c} = \frac{A\cos(\omega t)}{\omega CA\cos(\omega t - 90^\circ)} = \frac{\cos(\omega t)}{\omega C\cos(\omega t - 90^\circ)}$ 

A capacitor looks like a resistance whose magnitude goes as 1/ωC

A capacitor introduces a 90° phase difference between current and Voltage.





# Capacitors and Laplace

Let 
$$V(t) = Ae^{st}$$
  
 $\frac{dV}{dt} = sAe^{st}$   
Therefore  $i = sCAe^{st}$   
 $\frac{V}{i} = \frac{Ae^{st}}{sCAe^{st}}$   
 $= \frac{1}{sC}$ 

A capacitor acts like a resistance whose value depends on C and s!





# Capacitor Demo



 $C = \frac{\varepsilon_0 A}{D}$ 

Typical Tape Thickness ~5E-5 m

 $\varepsilon_0 \approx 8.854 \times 10^{-12}$  F/m



Center for Cognitive Neuroscience 16

# Laplace and Sinusoids

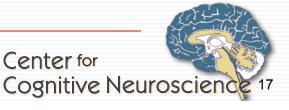
Through Euler's formula with  $s=i\omega$  (or  $j\omega$ ):  $Ae^{st} = Ae^{j\omega t} = A(\cos(\omega t) + j\sin(\omega t))$ 

Letting: 
$$V(t) = A\cos(\omega t)$$
  
=  $\Re[Ae^{j\omega t}]$ 

we see that:  $i_c = sCAe^{st} = j\omega CA(\cos(\omega t) + j\sin(\omega t))$ =  $j\omega CA\cos(\omega t) - \omega CA\sin(\omega t)$ 

Whose real part is simply  $i_c = -\omega CA \sin(\omega t)$  as before.





*Resistance* is the proportionality between constant current and constant Voltage.

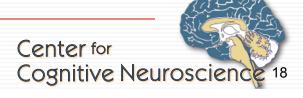
V = iR

*Impedance* is the ratio between time-varying Voltage and time-varying current.

 $\mathbf{V} = \mathbf{IZ}$ 

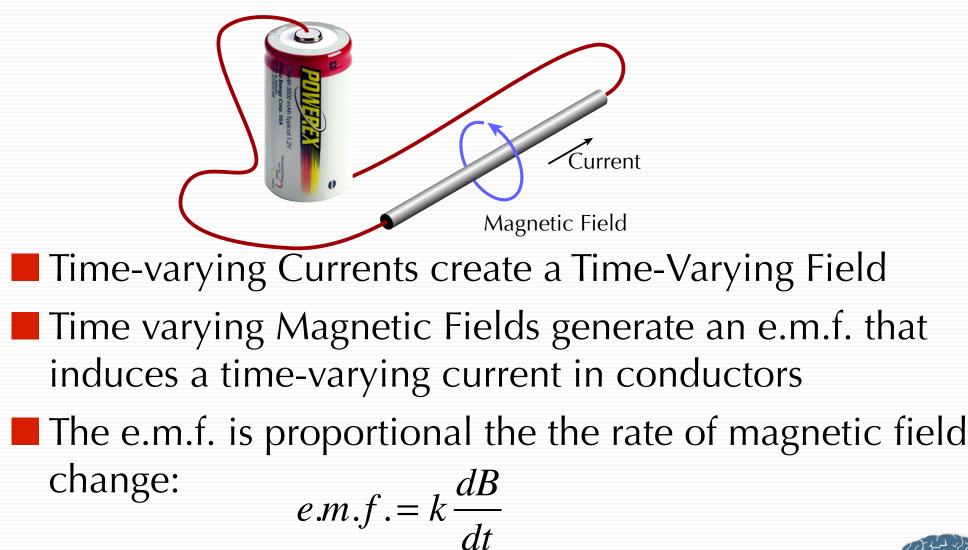
Noting that Z, I and V may be complex values
Z has a magnitude in Ohms, but may also include a phase.





### Inductance

Current creates a magnetic field about the conductor



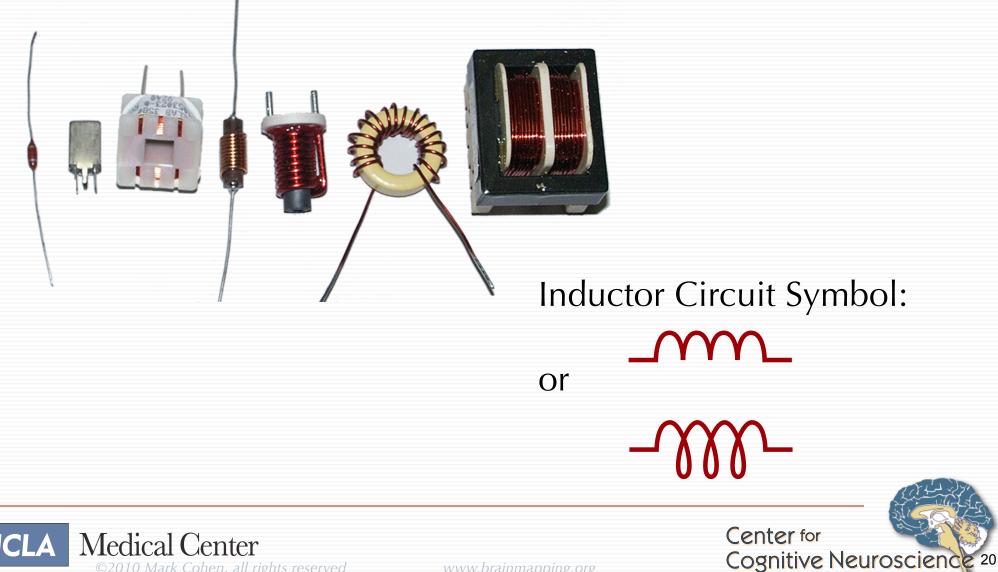


Center for

Cognitive Neuroscienc

### Inductors

Commercial Inductors are simply coils of wire.



©2010 Mark Cohen, all rights reserved

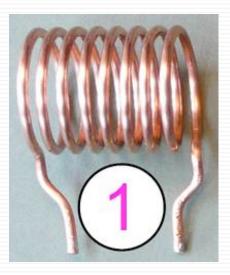
#### Inductors

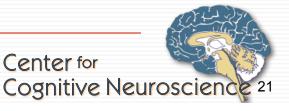
The magnetic field created by each loop of a coil is coupled to all of the other loops.

In general, the magnetic field created by a time-varying current opposes the same current flow in the other coils

The result is that:  
$$V_L = L \frac{di}{dt}$$

where is the voltage across the inductor and L is the inductance value (in Henries).





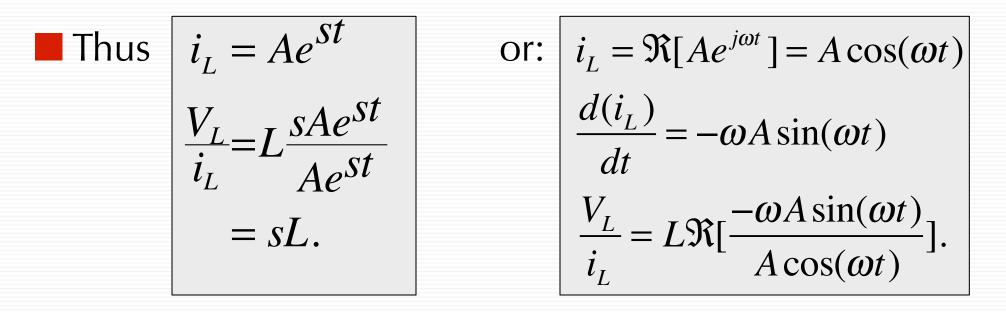
Frequency Characteristics of Inductors

Following the same reasoning as we used for a capacitor. Let:  $i = Ae^{st}$ , and  $s = j\omega$ 

$$V = sLAe^{st}$$

Medical Center

©2010 Mark Cohen, all rights reserved

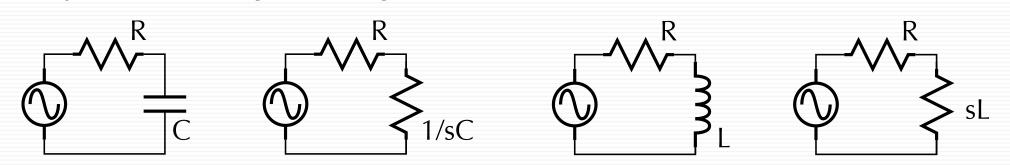


An inductor behaves like a resistor of magnitude sL that introduces a +90° phase shift.

> Center for Cognitive Neuroscience

# **Complex Impedance**

- Both Capacitors and Inductors have complex impedance: V/I is a complex quantity
- For a Capacitor, V/I=1/sC.
- For an Inductor, V/I=sL.
- In a circuit, we can replace all inductors and capacitors by their complex impedance:

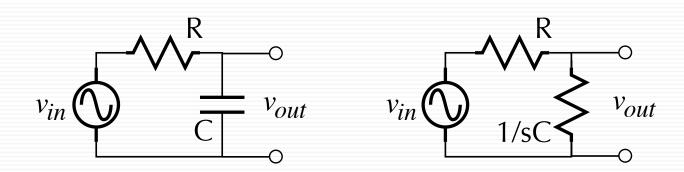


The circuits can then be analyzed with KVL and KCL

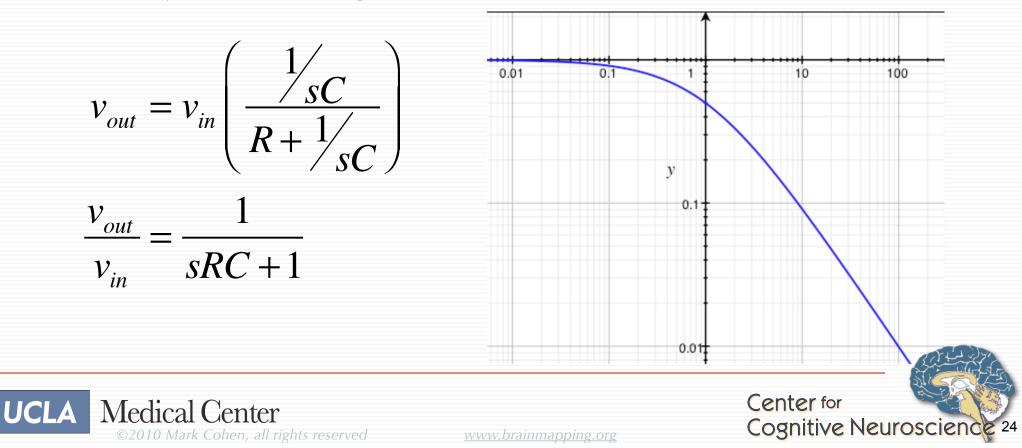


Center for Cognitive Neuroscience 23

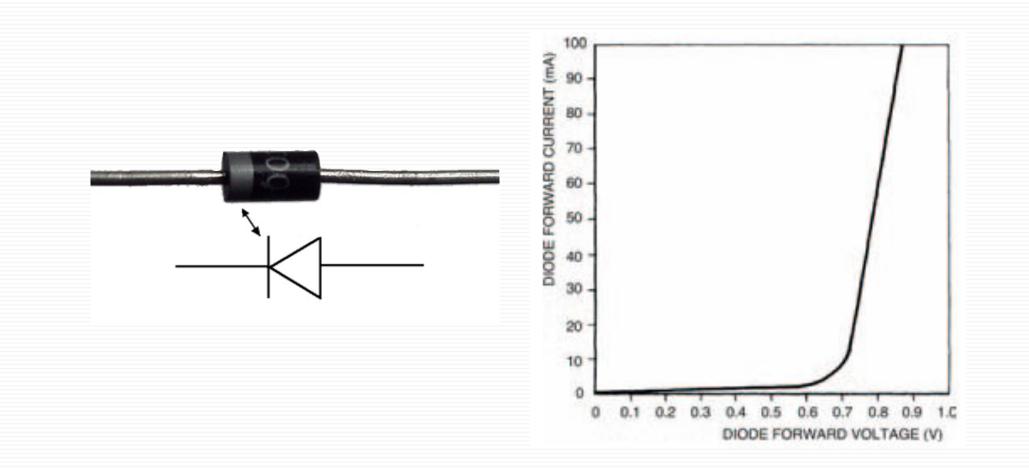
### Example



This is just a Voltage Divider circuit



### Diode





Center for Cognitive Neuroscience 25

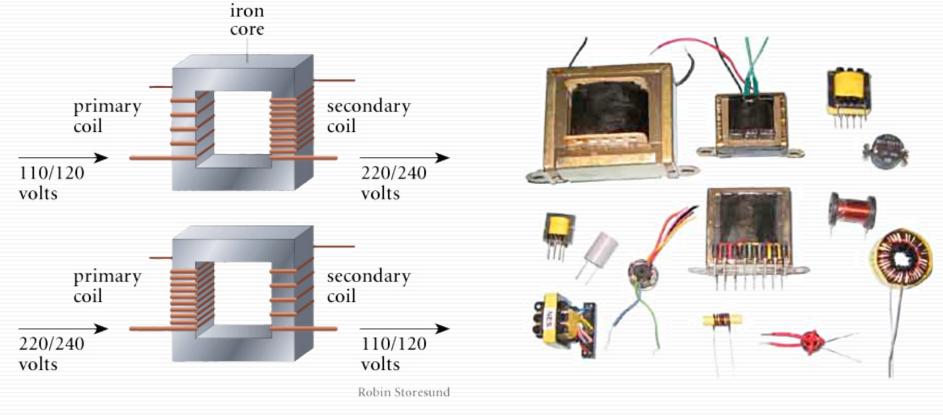
# Making Signals Bigger

Medical Center

©2010 Mark Cohen, all rights reserved

Physiological signals are too small to observe directly

Passive devices (transformer)



# Conservation of Energy: $v_{in}\dot{i}_{in} = v_{out}\dot{i}_{out}$

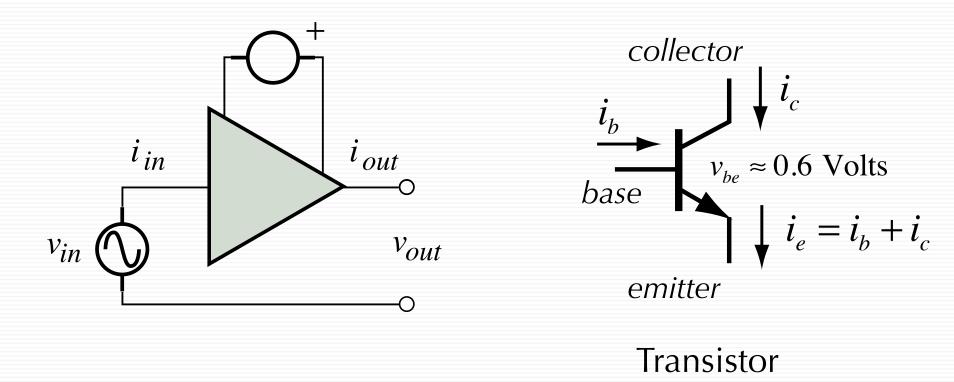


# Amplifiers

Generally: Total power is increased

$$v_{in}\dot{i}_{in} < v_{out}\dot{i}_{out}$$

Amplifiers require an added source of energy





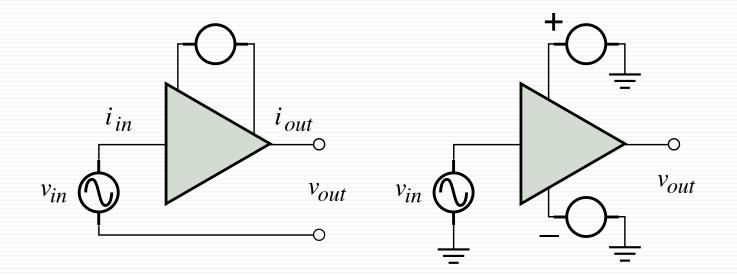
Center for Cognitive Neuroscience 27

### Ground

Ground is any selected node in a circuit

Usually, ground is selected as either one side of the input signal or the power supply.

All remaining Voltages are compared to Ground.





www.brainmapping.org

Center for

Cognitive Neuroscience 28

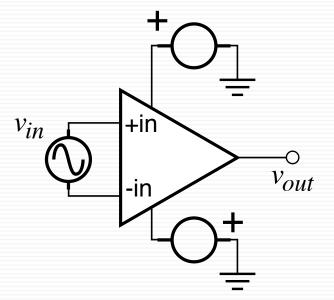
# **Operational Amplifier**

- Ideal Op Amp
  - 🖵 infinite gain
  - No current flows between +in and -in
- Real Op Amp
  - $\Box$  maximum output Voltage  $\approx$  the power supply
  - **g**ain > 1E4
  - $\Box$  input current << 1µA

**Medical** Center

©2010 Mark Cohen, all rights reserved

On the Op Amp: +, +in, v+ are used equivalently -, -in, v- are used equivalently





### Datasheet

#### TL081, TL081A, TL081B, TL082, TL082A, TL082B TL082Y, TL084, TL084A, TL084B, TL084Y JFET-INPUT OPERATIONAL AMPLIFIERS SLOS081E - FEBRUARY 1977 - REVISED FEBRUARY 1999

- Low Power Consumption
- Wide Common-Mode and Differential Voltage Ranges
- Low Input Bias and Offset Currents
- **Output Short-Circuit Protection**
- Low Total Harmonic Distortion . . . 0.003% Typ

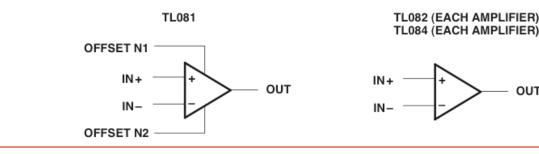
- High Input Impedance . . . JFET-Input Stage
- Latch-Up-Free Operation
- High Slew Rate . . . 13 V/us Typ
- Common-Mode Input Voltage Range Includes V<sub>CC+</sub>

#### description

The TL08x JFET-input operational amplifier family is designed to offer a wider selection than any previously developed operational amplifier family. Each of these JFET-input operational amplifiers incorporates well-matched, high-voltage JFET and bipolar transistors in a monolithic integrated circuit. The devices feature high slew rates, low input bias and offset currents, and low offset voltage temperature coefficient. Offset adjustment and external compensation options are available within the TL08x family.

The C-suffix devices are characterized for operation from 0°C to 70°C. The I-suffix devices are characterized for operation from -40°C to 85°C. The Q-suffix devices are characterized for operation from -40°C to 125°C. The M-suffix devices are characterized for operation over the full military temperature range of -55°C to 125°C.

#### symbols



Center for Cognitive Neuroscience

30

OUT

©2010 Mark Cohen, all rights reserved

Medical Center

# Datasheet (cont'd)

Medical Center

©2010 Mark Cohen, all rights reserved

UCLA

electrical characteristics,  $V_{CC\pm} = \pm 15 V$  (unless otherwise noted)

PARAMETER		TEST CONDITIONS		τ <sub>A</sub> †	TL081C TL082C TL084C			TL081AC TL082AC TL084AC			TLO81BC TL082BC TL084BC			TL081I TL082I TL084I			UNIT
					MIN	TYP	MAX	MIN	TYP	MAX	MIN	TYP	MAX	MIN	TYP	MAX	
V <sub>IO</sub> Input	Input offset voltage	V <sub>O</sub> = 0	R <sub>S</sub> = 50 Ω	25°C		3	15		3	6		2	3		3	6	mV
	input onset voltage		ng = 50 32	Full range			20			7.5			5			9	
αVIO	Temperature coefficient of input offset voltage	V <sub>O</sub> = 0	R <sub>S</sub> = 50 Ω	Full range		18			18			18			18		μV/°C
IIO	Input offset current‡	V <sub>O</sub> = 0		25°C		5	200		5	100		5	100		5	100	pА
				Full r						2			2			10	nA
1IB	Input bias current‡	VO = 0		- 2 4		30	4	00	30	200		30	200		30	200	pА
	input of ab our office	.0		Full ra					4	7			7			20	nA
VICR	Common-mode input voltage range			25°C	±11	-12 to		±11	-12 to		±11	-12 to		±11	-12 to		v
				200		15			15			15		± 11	15		ľ
VOM	Maximum peak output voltage swing	$R_L = 10 \ k\Omega$		25°C	±12	±13.5		±12	±13.5		±12	±13.5		±12	±13.5		
		$R_L \geq 10 \; k\Omega$		Full range	±12			±12			±12			±12			v
		$R_L \geq 2 \; k \Omega$							±12		±10	±12		±10	±12		
AVD	Large-signal differential voltage amplification	$V_{O} = \pm 10 V_{r}$	$R_L \geq 2  k \Omega$	2	5	20	0		200		50	200		50	200		
		$V_{O} = \pm 10 V_{,}$	$R_L \ge 2 k\Omega$	Full range				25			25			25			V/m\
B <sub>1</sub>	Unity-gain bandwidth			25°					3			3			3		MHz
ri	Input resistance			25°		10 <sup>12</sup>	2		1012			1012			1012		Ω
CMRR	Common-mode rejection ratio	$V_{IC} = V_{ICR}n$ $V_O = 0$ ,	nin, Rs = 50 Ω	25°C	70	00		75	86		75	86		75	86		dB
<sup>k</sup> SVR	Supply voltage rejection ratio (ΔV <sub>CC±</sub> /ΔV <sub>IO</sub> )	V <sub>CC</sub> = ±15 \ V <sub>O</sub> = 0,	/ to $\pm$ 9 V, R <sub>S</sub> = 50 $\Omega$	25°C	70	86		80	86		80	86		80	86		dB
ICC	Supply current (per amplifier)	$V_{O} = 0,$	No load	25°C		1.4	2.8		1.4	2.8		1.4	2.8		1.4	2.8	mA
V01/V02	Crosstalk attenuation	Avp = 100		25°C		120			120			120			120		dB

<sup>†</sup> All characteristics are measured under open-loop conditions with zero common-mode voltage unless otherwise specified. Full range for T<sub>A</sub> is 0°C to 70°C for TL08\_C, TL08\_AC, TL08\_BC and -40°C to 85°C for TL08\_I.

Input bias currents of a FET-input operational amplifier are normal junction reverse currents, which are temperature sensitive as shown in Figure 17. Pulse techniques must be used that maintain the junction temperature as close to the ambient temperature as possible.



#### TL081, TL081A, TL081B, TL082, TL082A, TL082B TL082Y, TL084, TL084A, TL084B, TL084Y JFET-INPUT OPERATIONAL AMPLIFIERS

SLOS081E – FEBRUARY 1977 – REVISED FEBRUARY 1999

#### absolute maximum ratings over operating free-air temperature range (unless otherwise noted)<sup>†</sup>

		TL08_C TL08_AC TL08_BC	TL08_I	TL084Q	TL08_M	UNIT		
Supply voltage, V <sub>CC+</sub> (see Note 1)	18	18	18	18	V			
Supply voltage V <sub>CC</sub> - (see Note 1)	-18	-18	-18	-18	V			
Differential input voltage, VID (see Note 2)	± 30	± 30	± 30	± 30	V			
Input voltage, VI (see Notes 1 and 3)	±15	±15	±15	±15	V			
Duration of output short circuit (see Note 4)	unlimited	unlimited	unlimited	unlimited				
Continuous total power dissipation	See Dissipation Rating Table							
Operating free-air temperature range, TA	0 to 70	- 40 to 85	- 40 to 125	– 55 to 125	°C			
Storage temperature range, Tstg	- 65 to 150	- 65 to 150	- 65 to 150	- 65 to 150	°C			
Case temperature for 60 seconds, T <sub>C</sub>	FK package				260	°C		
Lead temperature 1,6 mm (1/16 inch) from case for 60 seconds	J or JG package				300	°C		
Lead temperature 1,6 mm (1/16 inch) from case for 10 seconds	D, N, P, or PW package	260	260	260		°C		

<sup>†</sup> Stresses beyond those listed under "absolute maximum ratings" may cause permanent damage to the device. These are stress ratings only, and functional operation of the device at these or any other conditions beyond those indicated under "recommended operating conditions" is not implied. Exposure to absolute-maximum-rated conditions for extended periods may affect device reliability.

NOTES: 1. All voltage values, except differential voltages, are with respect to the midpoint between VCC+ and VCC-.

Differential voltages are at IN+ with respect to IN-.

2010 Mark Cohen, all rights reserved

Medical Center

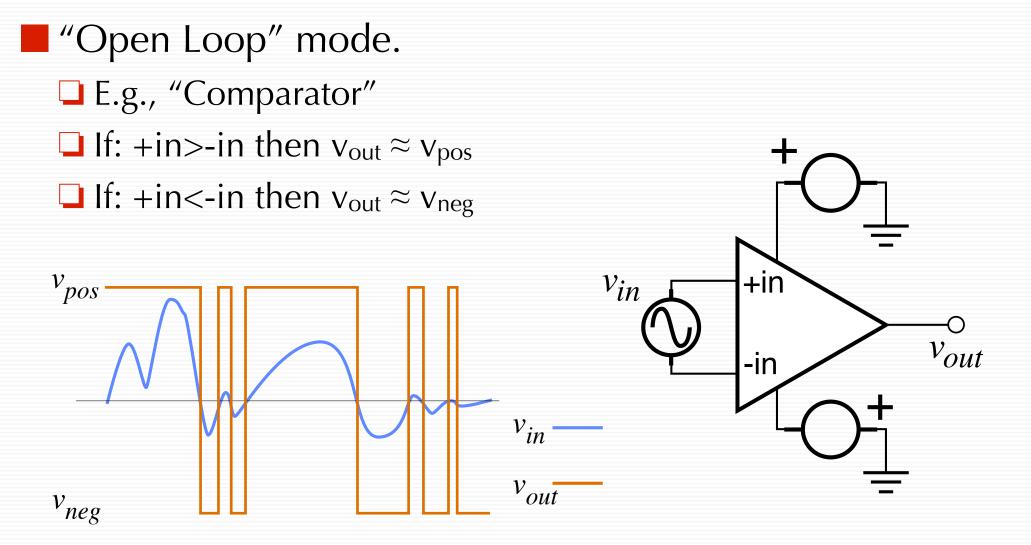
3. The magnitude of the input voltage must never exceed the magnitude of the supply voltage or 15 V, whichever is less.

4. The output may be shorted to ground or to either supply. Temperature and/or supply voltages must be limited to ensure that the dissipation rating is not exceeded.



Center for

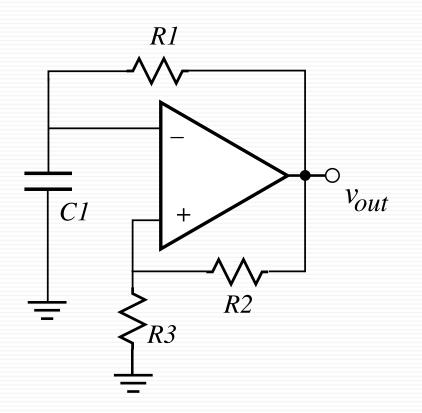
# Op Amp Non-linear Operation







# Multivibrator







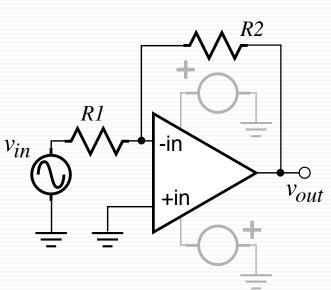
# Linear Operation for Op Amps

- Negative Feedback
- +in  $\approx$  -in
  - $-v_{cc} < v_{out} < +v_{cc}$
- Voltage at inverting (v-, or -in) and non-inverting (v+, or +in) inputs is equal.
- No current flows between these inputs
- $\mathbf{I}$   $v_{out}$  is adjusted as needed for the above to be true.





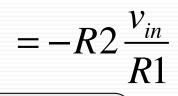
# **Inverting Amplifier**



In these slides, *-in* is the Voltage at the inverting input of the op amp (with respect to ground), and *+in* is the voltage at the non-inverting input.

In this circuit, negative feedback  $v_{R1} = v_{in}$ is used to ensure that  $v_{-}$  and  $v_{+}$ are kept equal. In this case, they  $i_{R1} = \frac{v_{in}}{R1}$ are kept at ground.

Because no current can flow between the inverting (–) and non-inverting (+) inputs to the op amp, the current through R2 must equal iR1. Therefore the Voltage across R2 must equal R2\* iR1. This Voltage must therefore be sourced by the output of the op amp:  $v_{out} = -i_{R1}R2$ 

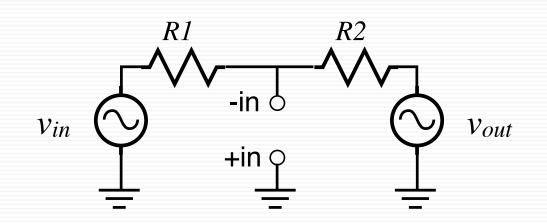


Cognitive Neuroscience 36

$$\frac{v_{out}}{v_{in}} = \frac{-R2}{R1}$$

Center for

## Inverting Amplifier Equivalent Circuit



In an op amp,  $v_{out}$  is controlled by the difference between -in and +in. The output Voltage is fed back (*negative feedback*) to the *v*- input so that the  $(+in - -in) \approx 0$ .

*No* current flows between +*in* and -*in* therefore, in this case, the current through R1 also goes through R2. The energy to supply that current is provided by the op amp (actually from its power supplies).

Notice the direction of the current through R2: when  $v_{in}$  is positive,  $v_{out}$  must be negative.

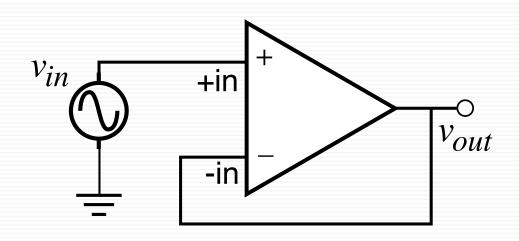
From the perspective of the input source, the op amp can be modeled as a resistor of value, R1.



Center for

Cognitive Neuroscienc

## Voltage Follower

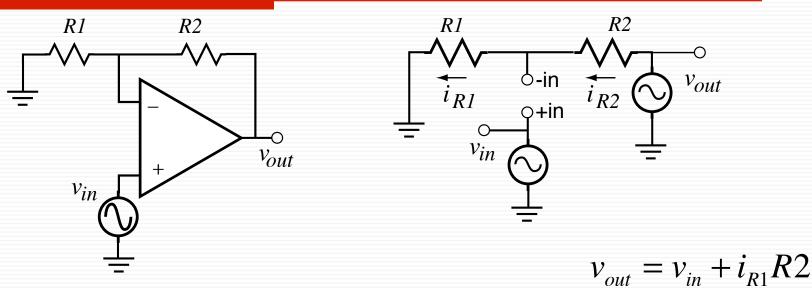


At first blush, this very common op amp circuit seems odd. After all, it is clear that if *-in* and *+in* are equal  $v_{out} = v_{in}$ .

What makes this useful, is that no matter what load  $v_{out}$  is connected to, the op amp ensures that no current flows into the +*in* input. The Voltage follower *isolates* the input source from the load driven by  $v_{out}$ . This means that the input source is not altered by driving a load. Essentially no current flows out of the input source (which therefore loses no energy).



#### Non-Inverting Amplifier



In this case the *-in* input is going to be set to  $v_{in}$  by the output Voltage source of the op amp. This means that  $v_{out}$  must be equal to the Voltage across R2, plus the Voltage across R1 (which is  $v_{in}$ ).

If  $v_{in}$  is positive the current flows in the direction shown. This means that  $v_{out}$  also is positive.

**Medical** Center

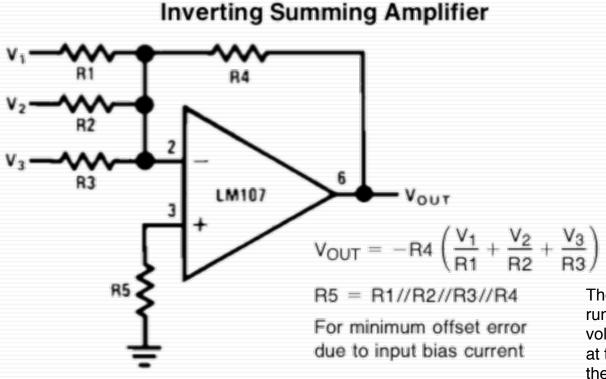
©2010 Mark Cohen, all rights reserved

 $= v_{in} + \frac{v_{in}}{R1}R2$  $= v_{in} \left(1 + \frac{R2}{R1}\right)$ 

$$\frac{v_{out}}{v_{in}} = 1 + \frac{R2}{R1} = \frac{R1 + R2}{R1}$$



## Inverting Summing Amplifier

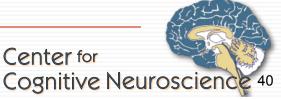


Medical Center

©2010 Mark Cohen, all rights reserved

The idea with R5 is that a small "bias" current must run into both Op amp inputs. To ensure that the voltages at both inputs are the same, the resistance at the inputs must be kept equal. Hence R5 is set to the equivalent parallel resistance of R1, R2 R3 and R4

# The current through R4 is equal to the sum of the currents through R1, R2 and R3 (*KCL*).



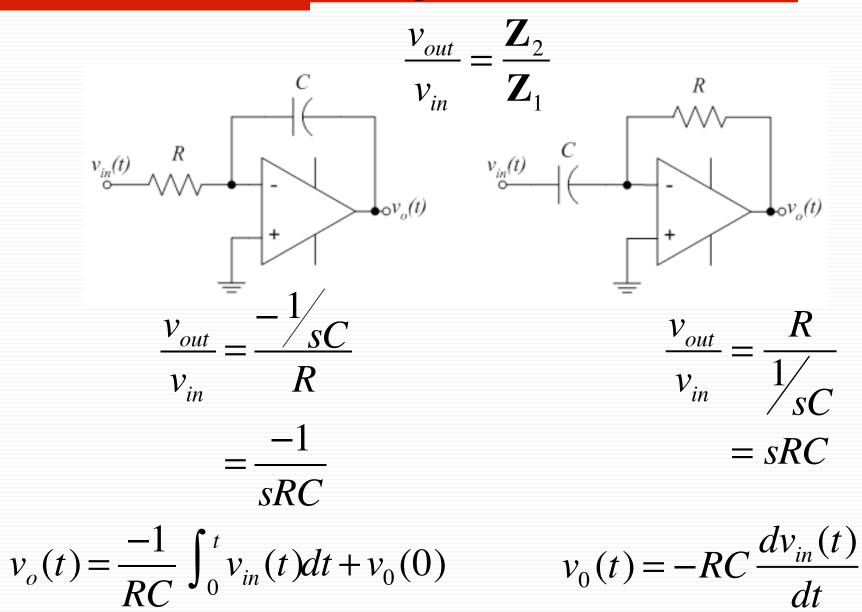
www.brainmapping

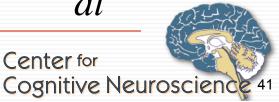
## Differentiator and Integrator

Medical Center

©2010 Mark Cohen, all rights reserved

UCL

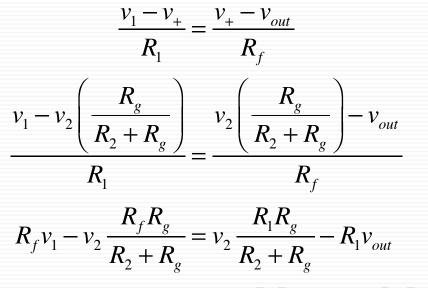




## **Difference** Amplifier

A "difference amplifier" amplifies the *difference* in voltage between to points, v1 and v2, rejecting any Voltage they have in common.

The current through R1, iR1, is (v1-v+)/R1, and is the same as the current through  $R_f$ , which is (v+-vout)/R2.



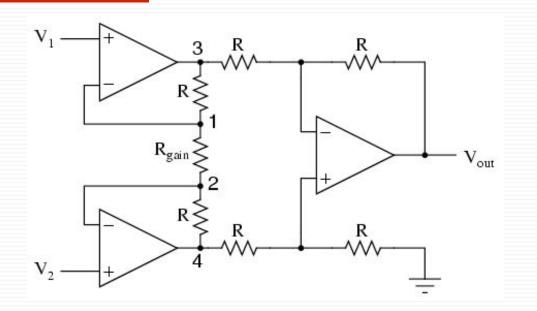
$$R_{1}v_{out} = v_{2}\frac{R_{1}R_{g}}{R_{2} + R_{g}} + v_{2}\frac{R_{f}R_{g}}{R_{2} + R_{g}} - R_{f}v$$

 $V_{\rm out}$ The Voltage divider at the non-inverting input *ensures* that:  $v_{+} = v_{2} \left( \frac{R_{g}}{R_{2} + R_{1}} \right).$  $v_{out} = v_2 \frac{R_g}{R_2 + R_c} + v_2 \frac{K_f K_g}{R_1 (R_2 + R_c)} - v_1 \frac{K_f}{R_1}$  $= v_2 \left( \frac{R_1 R_g}{R_1 (R_2 + R_1)} + \frac{R_f R_g}{R_1 (R_2 + R_2)} \right) - v_1 \frac{R_f}{R_1}$  $= v_2 \left( \frac{R_g \left( R_1 + R_f \right)}{R_1 \left( R_2 + R_o \right)} \right) - v_1 \frac{R_f}{R_1}$ If R<sub>1</sub>=R<sub>2</sub> and R<sub>f</sub>=R<sub>g</sub>:  $v_{out} = (v_2 - v_1) \frac{K_f}{R_1}$ 

Medical Center 010 Mark Cohen, all rights reserved

Center for Cognitive Neuroscience 42

#### Instrumentation Amplifier



An instrumentation amplifier is essentially a difference amplifier whose inputs are isolated from the source by Voltage followers. Virtually no current flows between  $v_1$  and  $v_2$ .

Why? Because any difference in Voltage between the  $v_1$  and  $v_2$  terminals of the first op amps must be matched by the Voltage across the two v- terminals. This appears across R3. The current to produce this drop must come through the two R2 resistors. If they are large that current will create a large Voltage across them.



#### Integrated Instrumentation Amplifier

#### FEATURES

- LOW OFFSET VOLTAGE: 50µV max
- LOW DRIFT: 0.25µV/°C max
- LOW INPUT BIAS CURRENT: 2nA max
- HIGH COMMON-MODE REJECTION: 115dB min
- INPUT OVER-VOLTAGE PROTECTION: ±40V
- WIDE SUPPLY RANGE: ±2.25 to ±18V
- LOW QUIESCENT CURRENT: 3mA max
- 8-PIN PLASTIC AND SOL-16

#### APPLICATIONS

- BRIDGE AMPLIFIER
- THERMOCOUPLE AMPLIFIER
- RTD SENSOR AMPLIFIER
- MEDICAL INSTRUMENTATION
- DATA ACQUISITION

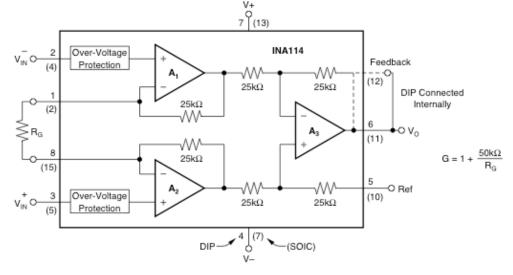
#### DESCRIPTION

The INA114 is a low cost, general purpose instrumentation amplifier offering excellent accuracy. Its versatile 3-op amp design and small size make it ideal for a wide range of applications.

A single external resistor sets any gain from 1 to 10,000. Internal input protection can withstand up to  $\pm 40V$  without damage.

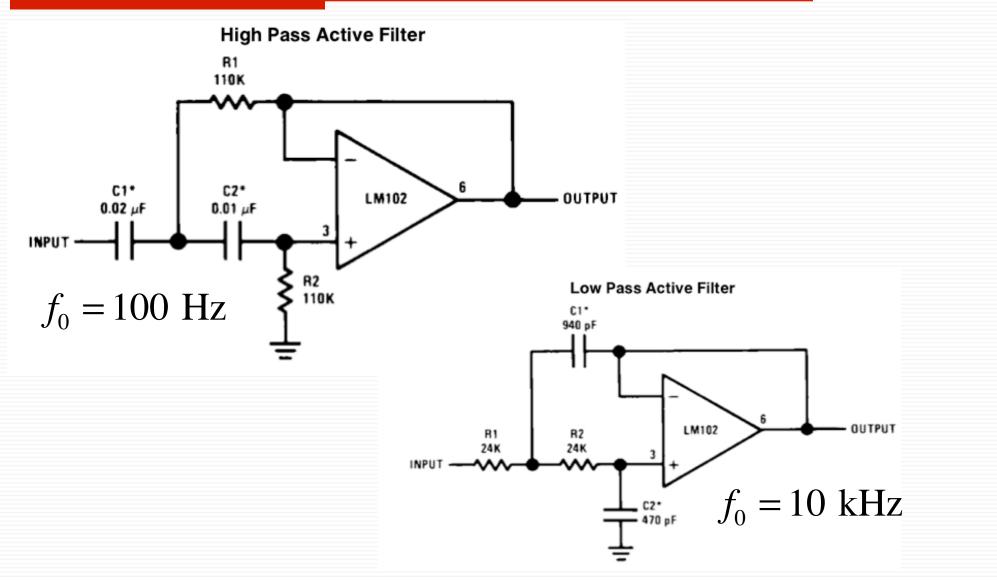
The INA114 is laser trimmed for very low offset voltage (50 $\mu$ V), drift (0.25 $\mu$ V/°C) and high common-mode rejection (115dB at G = 1000). It operates with power supplies as low as ±2.25V, allowing use in battery operated and single 5V supply systems. Quiescent current is 3mA maximum.

The INA114 is available in 8-pin plastic and SOL-16 surface-mount packages. Both are specified for the -40°C to +85°C temperature range. By making the amplifier on a single piece of silicon, the manufacturer can ensure that all of the resistors are matched precisely. In turn, this makes sure that common mode signals are heavily attenuated.



Center for Cognitive Neuroscience

## Second Order Filter



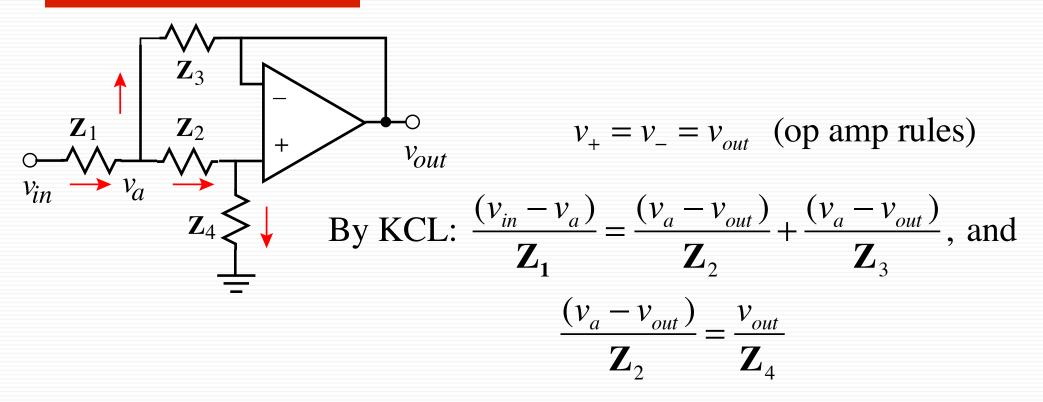


www.brainmapping.org

Center for

Cognitive Neuroscience 45

#### Second Order Filter Analysis



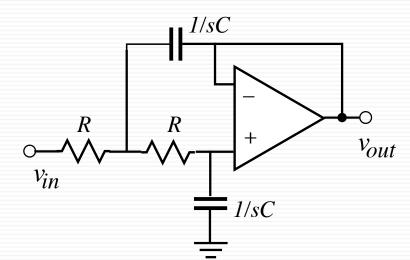
Although the algebra is tedious, these can be solved for  $v_{out}/v_{in}$ :

$$\frac{v_{out}}{v_{in}} = \frac{\mathbf{Z}_3 \mathbf{Z}_4}{\mathbf{Z}_3 \mathbf{Z}_4 + \mathbf{Z}_2 \mathbf{Z}_3 + \mathbf{Z}_1 \mathbf{Z}_3 + \mathbf{Z}_1 \mathbf{Z}_2}$$

Center for Cognitive Neuroscience 46

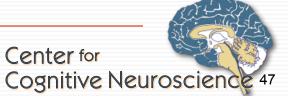


#### Low Pass Filter

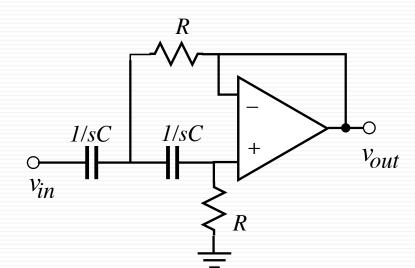


$$\frac{v_{out}}{v_{in}} = \frac{\mathbf{Z}_{3}\mathbf{Z}_{4}}{\mathbf{Z}_{3}\mathbf{Z}_{4} + \mathbf{Z}_{2}\mathbf{Z}_{3} + \mathbf{Z}_{1}\mathbf{Z}_{3} + \mathbf{Z}_{1}\mathbf{Z}_{2}}$$
$$\mathbf{Z}_{1} = \mathbf{Z}_{2} = R, \quad \mathbf{Z}_{3} = \mathbf{Z}_{4} = \frac{1}{sC}$$
$$\frac{v_{out}}{v_{in}} = \frac{\frac{1}{s^{2}C^{2}}}{\frac{1}{s^{2}C^{2}} + \frac{R}{sC} + \frac{R}{sC} + R^{2}}$$
$$= \frac{1}{1 + 2sRC + s^{2}R^{2}C^{2}} = \frac{1}{(1 + sRC)^{2}}$$

UCLA Medical Center ©2010 Mark Cohen, all rights reserved



High Pass Filter



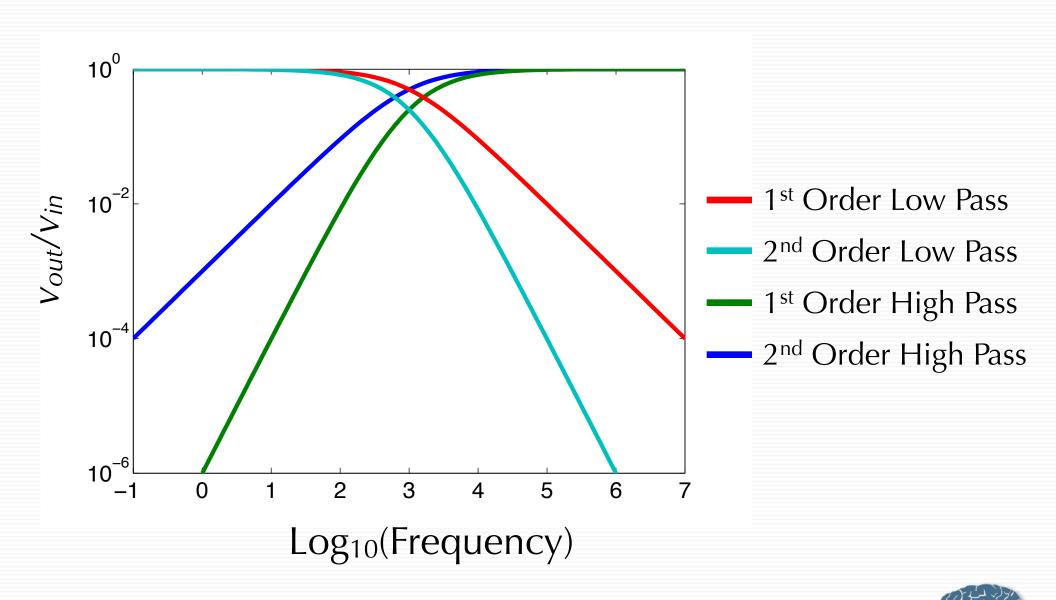
$$\frac{P_{in}}{P_{in}} = \frac{R^2}{R^2 + \frac{R}{sC} + \frac{R}{sC} + \frac{1}{s^2C^2}}$$
$$= \frac{R^2 s^2 C^2}{1 + 2sRC + s^2 R^2 C^2} = \frac{(sRC)^2}{(1 + sRC)^2}$$

Center for

Cognitive Neuroscience 48

UCLA Medical Center ©2010 Mark Cohen, all rights reserved

#### First and Second Order Filters





www.brainmapping.org

Center for

Cognitive Neuroscience 49